







# Research and networking activities at the LNL laboratories

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MidiNet task 2. Mid term meeting Београд, 12-14 March 2018

### Microdosimetric Study with the CNAO Active-Scanning Carbon-Ion Beam doi:10.1093/rpd/ncx217





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### Two detectors were used



The mini Tissue-Equivalent Proportional Counter (mini-TEPC). LNL-INFN



#### *The silicon microdosimeter. Politecnico of Milano*



More than 7000 pixels are connected in parallel to give an effective detection area of the  $\Delta E$  stage of about 0.3  $mm^2$ 





### Measurements were performed inside a water phantom







## ACTIVE SCANNING: 225 beam spots of 6 mm of diameter uniformly fill the area





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MediNet <u>Task 2</u>

### **Relative mean values comparison: relative dose**





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## Relative mean values comparison: saturation-corrected $\bar{y}_{D}$



ICRU report 36. 1983



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## Microdosimetric inter-comparison with the 62 MeV/u carbon-ion beam of Catania

submitted to Physica Medica



Mini-TEPC LNL-INFN





Diamond detector Roma2-INFN, MedAustron

#### Silicon detector Polimi





### The beam line of LNS laboratory and the PMMA phantom







## Relative dose, points of the measurements and averaged dose-mean LET





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## The response of the four detectors at 7.9 mm of water-equivalent depth







## $\overline{y}_{D}$ -values inter-comparison and $\overline{LET}_{D}$







## $\overline{y}_{D}$ against $\overline{LET}_{D}$ at different depths



## The microdosimeter is a LET counter only as a first approximation,

In a mixed-radiation field different particle tracks have different LET (L) values. They give rise to the distribution t(L), which is different from the f(y) distribution. However, the respective momenta are proportional when the particles cross randomly the detector in CSDA:

$$\overline{y^n} = \frac{\overline{l^n}}{\overline{l}^n} \cdot \overline{L^n}$$

Therefore for any detector:

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$$\overline{y}_F = \overline{L}_F$$
 and  $\overline{y}_D \neq \overline{L}_D$ 

If we consider the energy straggling, we have:

$$\overline{y}_D = \frac{\overline{l^2}}{\overline{l^2}} \cdot \overline{L}_D + \frac{\overline{E}_w}{\overline{l}}$$

Where  $E_w$  is the weighted mean of the collision spectrum

A.M.Kellerer in Second Symposium on Microdosimetry EUR 4452 d-f-e-, 107-135

P.Colautti. Detectors for Radiation Quality in Ion-Beam Therapy . LNL 30-31 January 2017 MediNet

## CONCLUSIONS

The scientific collaboration is continuing with:

- 1. INFN laboratories of Catania, Italy
- 2. INFN section of Padova, Italy
- 3. Politecnico of Milano, Italy
- 4. University of Roma 2, Italy
- 5. MedAustron, Austria
- 6. FCK•CEN of Mol, Belgium
- 7. University of Hasselt, Belgium
- 8. ELI-Beamlines. Dolní Břežany, Czech Republic.
- 9. ELI- National Physical Laboratory, Teddington, UK.
- 10.CNAO, Pavia, Italy

With the aim of constructing reliabile microdosimeters operative in the clinic environment.





## The microdosimeter is also, as a first approximation, a LET counter

In a mixed-radiation field different particle tracks have different LET (L) values. They give rise to the distribution t(L), which is different from the f(y) distribution. In CSDA, when the particles cross randomly the detector :

$$\overline{L^n} = \frac{\overline{l}^n}{\overline{l^n}} \cdot \overline{y^n}$$

Therefore:

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 $\overline{L}_F = \overline{y}_F$  and  $\overline{L}_D \neq \overline{y}_D$ 

If we include the energy straggling of the particle:

$$\overline{L}_D = \frac{\overline{l}^2}{\overline{l^2}} \cdot \overline{y}_D - \frac{\overline{l}}{\overline{l_2}} \cdot \overline{E}_w$$

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